

A2V: A Semi-Supervised Domain Adaptation Framework for Brain Vessel Segmentation via Two-Phase Training Angiography-to-Venography Translation

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Context & Objectives

Anatomical differences between arteries and veins results in a **large domain gap**.

Domain Adaptation (DA) tackles the problem of distribution shifts across image modalities. However:

- **Small objects** are not preserved during translation.
 - Vessels are merged with the background.
- **Label-altering features** are erroneously translated.
 - Vessels are changed in size or position.
- Arteries and veins are **not linked** during translation.
 - Vessels are left untransformed, thus not segmented.

We introduce a **semi-supervised DA framework** for segmenting brain veins using primarily annotated angiographies. We combine image translation and semantic segmentation by relying on a combined and disentangled latent representation.

Method

Setup: Images x_i from source domain \mathcal{S} and target domain \mathcal{T} are fed into our model, composed of:

- a generator G
- a discriminator D
- an encoder E

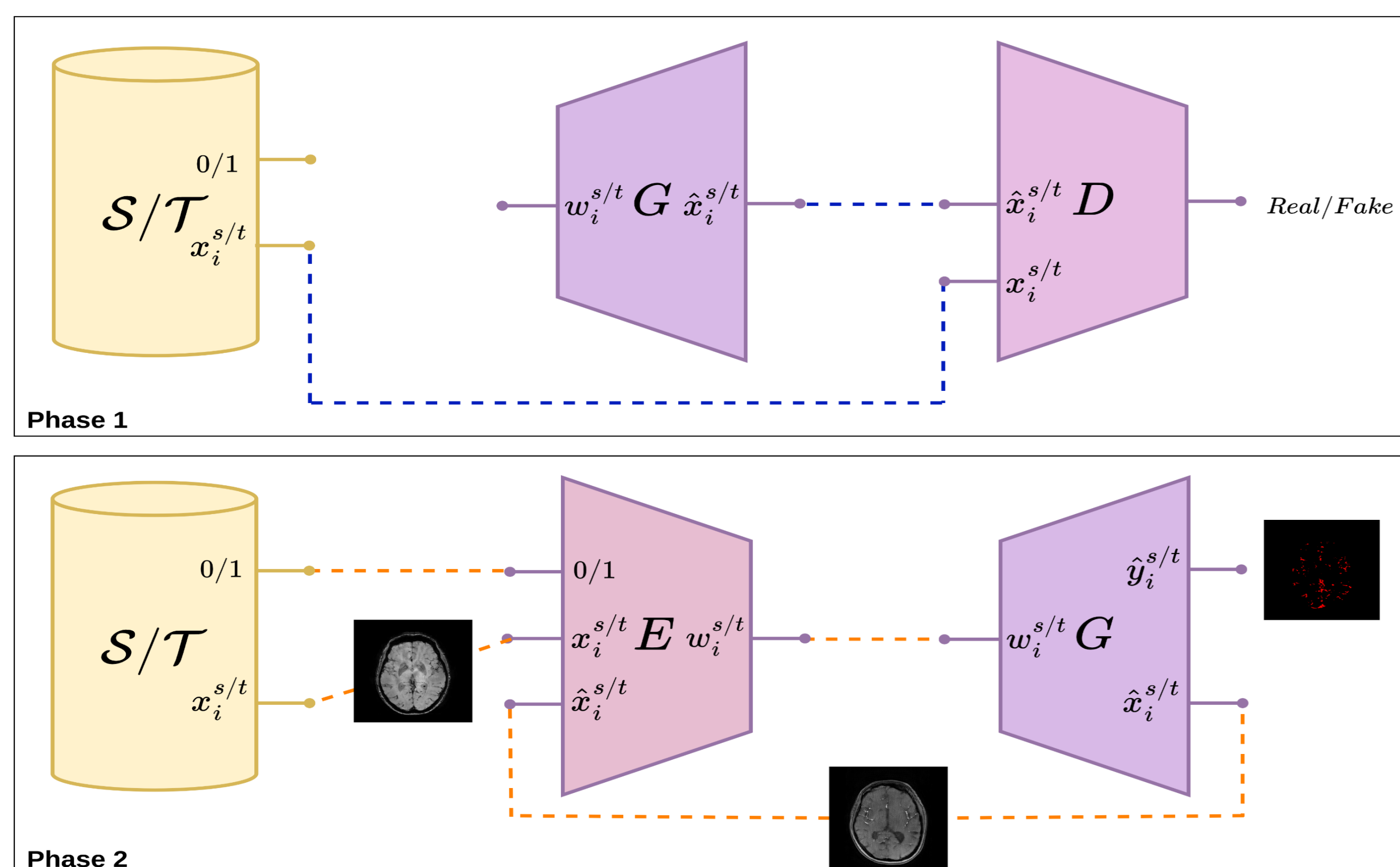


Fig 1. Two-phase training algorithm.

The modules are trained in two separate phases.

Phase 1: G maps latent vectors $w_i \in \mathcal{W}$ into an x_i , in \mathcal{S} or \mathcal{T} . D discriminates real and fake samples.

Disentanglement guarantees label-preserving translation between the two domains. Hence, E can handle individual features independently from others, discovering high-level mappings that differentiate between various vessel characteristics. This allows to alter vessel intensities, while preserving compromising **volume-related** and **vessel-related** properties, such as image spacing or vessel arrangement.

Phase 2: E reconstructs or transforms an image in \mathcal{S} and \mathcal{T} . G has a label-synthesis branch for segmentation.

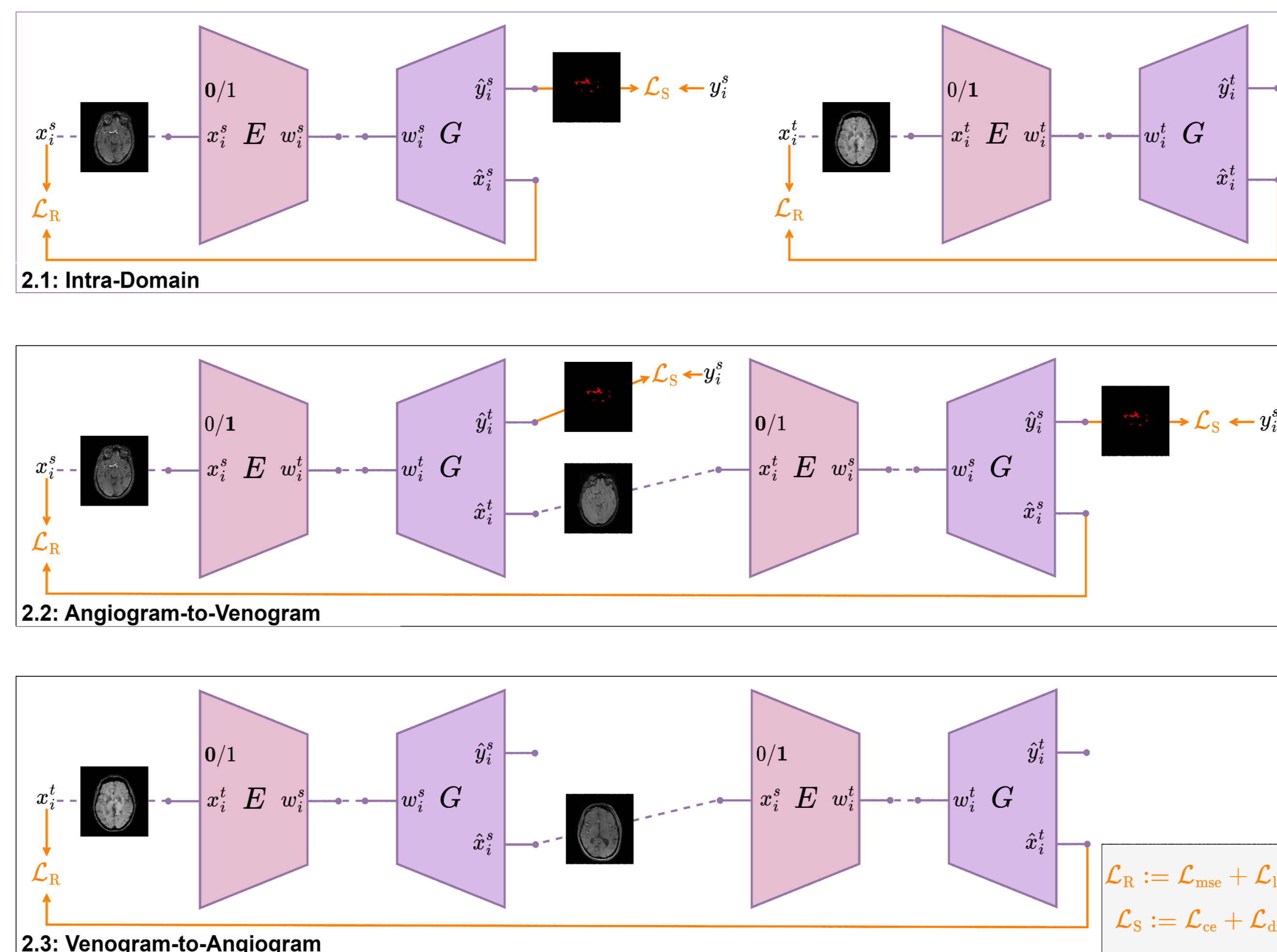


Fig 2. Phase 2 of the training algorithm alternating intra-domain (2.1) and inter-domain (2.2 and 2.3) configurations

Experiments & Results

We used **time-of-flight MR** angiographies as \mathcal{S} , and **susceptibility weighted imaging** venographies as \mathcal{T} .

Method*	Brain Dice	Vessels Dice	Vessels cIDice
SIFA	91.5 ± 0.4	0.8 ± 0.2	0.8 ± 0.2
SynthSeg	79.6 ± 3.8	37.3 ± 4.4	48.2 ± 4.7
CS-CADA	91.5 ± 0.8	51.4 ± 1.7	58.0 ± 2.8
DCDA	-	4.5 ± 0.4	3.9 ± 0.2)
Sato	-	44.2 ± 7.2	50.0 ± 6.7
Ours	97.5 ± 0.2	70.4 ± 2.4	74.8 ± 2.4

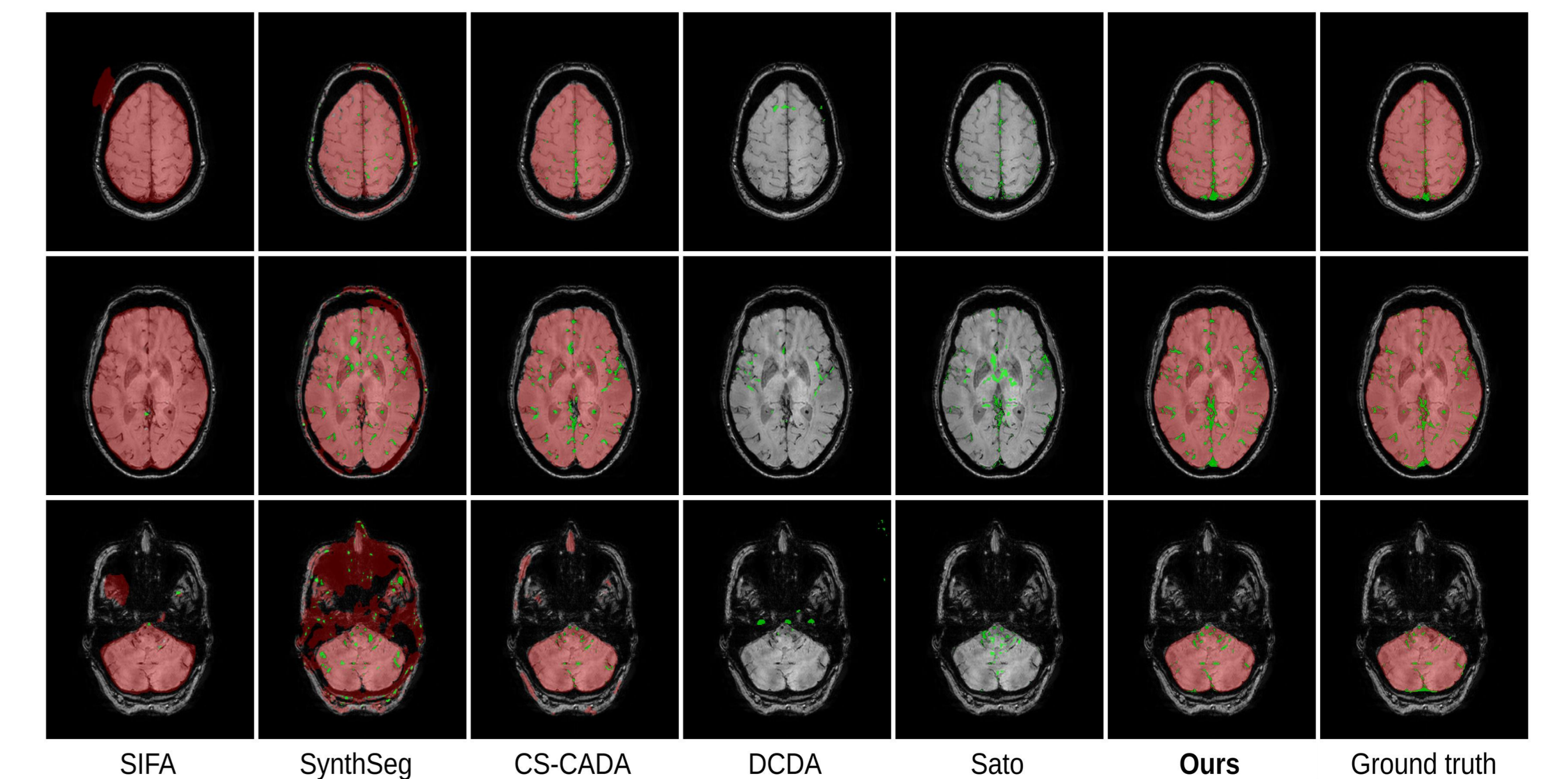


Fig 3. Visual comparison.

Conclusions

- **Accurate** segmentation of 3D brain vessels using primarily annotations from arterial images.
- **Optimized** cycle-based network, counting two essential components, G and E .
- **Two-phase** learning algorithm, guaranteeing that only D is involved with adversarial training, and discarded after Phase 1.
- Code **freely available**:

